Prefrontal synaptic activation during hippocampal memory reactivation

Graphical abstract

Highlights
- Simultaneous multiunit recordings and whole-cell recordings are performed
- Prefrontal neurons depolarize during hippocampal place cell synchronization
- Hippocampal-prefrontal associations depend on memory-related spike patterns

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In brief
Nishimura et al. find that medial prefrontal neurons receive depolarizing synaptic potentials when hippocampal place cells show synchronized spikes. This study provides direct physiological evidence of functional synaptic transmission from memory-encoding hippocampal neurons to prefrontal neurons.
Prefrontal synaptic activation during hippocampal memory reactivation

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SUMMARY

Cooperative reactivation of hippocampal and prefrontal neurons is considered crucial for mnemonic processes. To directly record synaptic substances supporting the interregional interactions, we develop concurrent spike recordings of hippocampal neuronal ensembles and whole-cell patch-clamp recordings of medial prefrontal neurons in awake rats. We find that medial prefrontal neurons depolarize when hippocampal neurons synchronize. The depolarization in medial prefrontal neurons is larger when hippocampal place cells that encoded overlapping place fields and place cells that encoded a novel environment are synchronously reactivated. Our results suggest a functional circuit-synapse association that enables prefrontal neurons to read out specific memory traces from the hippocampus.

INTRODUCTION

A functional information transfer from the hippocampus (HPC) to the prefrontal cortex (PFC), via direct and indirect synaptic projections (Cenquizca and Swanson, 2007; Hoover and Vertes, 2007; Spellman et al., 2015), is pivotal to declarative memories (Eichenbaum, 2017; Tang and Jadhav, 2019). A possible neurophysiological substrate for the HPC-PFC communication is the reactivation of HPC neuronal ensembles that encoded previously experienced behavioral trajectories (Joo and Frank, 2018; Lee and Wilson, 2002; Wilson and McNaughton, 1994), typically associated with sharp-wave ripples (SWRs), a high-frequency oscillation event (150–250 Hz) in local field potential (LFP) signals (Buzsáki, 2015). The roles of HPC synchronized activity in memory functions are supported by the observations that memory-related behavioral performance is improved by optogenetic prolongation of awake HPC SWRs (Fernández-Ruiz et al., 2019) and impaired by selective disruption of awake (Gridchyn et al., 2020; Igata et al., 2021; Jadhav et al., 2012) and sleep (Girardeau et al., 2009) HPC SWRs. For widespread cortical regions outside the HPC, the strong excitation gain during HPC SWRs is suited to drive pronounced changes in ongoing neuronal activity, possibly serving as a substrate for inter-regional information transfer (Logothetis et al., 2012; Vaz et al., 2019). Several studies have shown that HPC SWRs can encode coordinated reactivation of HPC-PFC cell ensembles that encode behaviorally relevant information (Benchenane et al., 2010; Jadhav et al., 2016; Peyrache et al., 2009; Shin et al., 2019), while a recent study questioned this view by demonstrating that replay of animals’ behavioral trajectories occurs almost independently between the HPC and the PFC (Kaefer et al., 2020), suggesting that this inter-regional information transfer is more complex than previously thought. While the precise HPC-PFC neuronal coordination is still under debate, it has been demonstrated at behavioral levels that reinforcing the HPC-PFC coordination during post-task periods facilitates memory consolidation (Maingret et al., 2016), which is suggestive of their potential roles in the redistribution of HPC labile mnemonic information into PFC long-term memory (Frankland and Bontempi, 2005; Tonegawa et al., 2018). For PFC neurons to efficiently read out information contents arising from the HPC, synchronized HPC cell ensemble patterns need to be properly transformed into synaptic inputs onto PFC neurons. The selective depolarization in a subset of PFC neurons then determines whether they participate in HPC-PFC coordinated activity. However, such neuronal inputs at a subthreshold level have not been directly measured, primarily owing to a lack of methodologies. To address this question, we simultaneously measured spike patterns of a HPC cell ensemble and a membrane potential of a medial PFC (mPFC) neuron from an awake rat by an integrated technique. While the ventral and intermediate HPC have been reported to more strongly project to the mPFC (Cenquizca and Swanson, 2007; Hoover and Vertes, 2007; Jay and Witter, 1991; Spellman et al., 2015) compared with the dorsal HPC, we recorded dorsal HPC neurons due to a technical limitation of recordings of sufficient numbers of HPC neuronal ensembles from the ventral and

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intermediate HPC. Thus, our results of the dorsal HPC-PFC interactions could be explained by indirect polysynaptic pathways through several brain areas such as the ventral HPC, thalamus, and neocortex.

RESULTS

Concurrent HPC multiunit recordings and mPFC whole-cell recordings

Rats were implanted with eight tetrodes directed at the HPC with a craniotomy over the mPFC for subsequent patch-clamp recordings (Figure S1A). During 2- to 3-week-post-surgery periods in which the tetrodes were lowered to the dorsal HPC pyramidal cell layer, the rats were trained to continuously run on a U-track to obtain a chocolate milk reward at both ends of the track and habituated to head restraint for subsequent patch-clamp recordings (Figure 1A). On a recording day, spike patterns were recorded from HPC putative pyramidal neurons in a 10- to 15-min familiar U-track task (Figure 1B). The well-trained rats completed 30.0 ± 2.5 running laps during a 10-min task period (n = 16 rats). A total of 135 HPC neurons were recorded. The majority of neurons were recorded from the CA1 area, whereas the minority of neurons were recorded from the CA2 area (Figure S2A). Of 84 place cells identified, 37 (44.1%) and 47 (55.9%) cells had unidirectional place fields depending on running direction and bidirectional place fields independent of running directions, respectively (Figures 1C and S3A–S3D). The rats were then head-fixed under awake conditions, and whole-cell recordings were obtained from electrophysiologically and morphologically identified pyramidal neurons in layers 2–5 of the mPFC (n = 18 cells from 16 rats; Figures 1B, S2B, and S2E). Minimizing physical damage from surgical procedures and restricting time periods of all these experimental procedures within 2 h enabled continuous tracking of spikes of identical HPC cells (Figures 1D and S2C). In the post-task head-fixed periods, mPFC LFP signals did not contain apparent slow, delta, and spindle oscillations (Figures S1C and S1D) (Maingret et al., 2016; Peyrache et al., 2009; Siapas and Wilson, 1998; Sirota et al., 2003), demonstrating that the rats were in awake quiescent states but not sleep states.

Synchronized reactivation of HPC neurons and mPFC membrane potentials

During whole-cell recordings from mPFC neurons, HPC neurons were synchronously reactivated (Figures 2A and S3E–S3G), consistent with previous studies (Eschenko et al., 2008; Kudrimoti et al., 1999; Norimoto et al., 2018). Based on the length of SWR-associated sequential replays reported previously (Buzsáki, 2015; Carr et al., 2011) and sufficient sample numbers of synchronous events in our datasets (Figures S3E–S3G and
S4J), we here used a time window of 100 ms to define HPC synchronization events. We assessed whether these HPC synchronization events impacted subthreshold potentials of mPFC neurons. For each mPFC neuron, distributions of mPFC membrane potential changes ($\Delta V_m$) were analyzed for different numbers of HPC synchronized cells ($N_{sync}$), ranging from 2 to 5 cells (an example mPFC neuron is shown in Figure 2B).

Assuming that the majority of HPC reactivation ranges within 100 ms and leads over mPFC activity by tens of milliseconds (Peyrache et al., 2009; Place et al., 2016), mPFC $\Delta V_m$ was computed from a post-event 0-to-150-ms time window after the onset of HPC synchronization. Here, HPC synchronization was independently computed by a comparison between real and surrogate distributions by the Kolmogorov-Smirnov test. Red dots show statistically significant results.

Figure 2. Prediction of a mPFC neuronal membrane potential from synchronized spikes of HPC neurons
(A) Simultaneous recordings of spike patterns of HPC neurons (top), the numbers of co-active HPC neurons (middle), and subthreshold $V_m$ in a mPFC neuron (bottom). Spikes were truncated for better visualization.
(B) (Top) Membrane potential traces of a representative mPFC neuron aligned to the time of synchronous firing of two ($N_{sync} = 2$), four ($N_{sync} = 4$), and five ($N_{sync} = 5$) HPC neurons. Individual traces are shown by thin gray lines, and the averages and SEM are shown by thick blue lines and thin blue regions, respectively. (Bottom) Distribution of membrane potential changes in the mPFC neuron at individual HPC synchronized events. The real distributions were compared with those in the corresponding surrogates in which the time of HPC synchrony was randomly shuffled (green lines).
(C) Shifts in average mPFC $\Delta V_m$ against the number of synchronized HPC neurons ($n = 13$ mPFC neurons from 13 rats with $>4$ HPC cells). Each line represents a recording from a mPFC neuron. The example mPFC neuron shown in (B) is highlighted by the orange line. For each plot at each $N_{sync}$ and at each mPFC, a p value was independently computed by a comparison between real and surrogate distributions by the Kolmogorov-Smirnov test. Red dots show statistically significant results.
(D) (Top) For a representative mPFC neuron from a rat (rat #59), a linear regression analysis was applied to predict mPFC $\Delta V_m$ at the time of each HPC synchrony from synchronized spike patterns of HPC cells (blue, observed; magenta, predicted). (Bottom) An error of prediction from the real data (black arrow) was compared with errors (in mV) of prediction from surrogate datasets in which observed $\Delta V_m$ were randomly shuffled across HPC synchrony (gray distribution). A prediction score was computed as a negative value of a Z score defined by the surrogate distribution. (Right) Distribution of weight for each cell used for the prediction. Red and blue edges represent positive and negative relationships with mPFC $\Delta V_m$, respectively.
(E) Membrane potential traces of the mPFC neuron aligned to the time of synchronous spikes of HPC neurons indicated. Individual traces are shown by thin gray lines, and the averages and SEM are shown by thick blue lines and thin blue regions, respectively.
(F) As in the bottom panel of (D), but for the other two mPFC neurons from two rats.
(G) Prediction scores of all 13 mPFC neurons (from 13 rats) plotted against the number of HPC neurons. Significantly predicted fractions with p < 0.05 defined by prediction scores are shown above the dotted line.
(H) Distribution of weight values of individual HPC neurons plotted against their firing rates in rats with significant prediction scores ($n = 43$ HPC cells from 5 rats). $R = -0.072$, $p = 0.60$.

See also Figure S4.
events that occurred within 200 ms from prior HPC SWRs were excluded from our analysis, as they potentially represented the second and subsequent events involved in ripple bursts (Yamamoto and Tonegawa, 2017). In the example mPFC neuron in Figure 2B, mPFC \( \Delta V_m \) distributions for \( N_{sync} \) of 3–5, but not for 2, showed significant rightward (depolarizing) shifts, compared with surrogate distributions in which each mPFC \( \Delta V_m \) was randomly extracted from the same mPFC membrane voltage trace, demonstrating that larger mPFC depolarization occurred significantly more often than by chance. Results from all mPFC neurons are summarized in Figure 2C (\( n = 13 \) mPFC neurons from 13 rats with >4 HPC neurons), in which each line represents each mPFC neuron, and each red dot indicates the average of a distribution with a significant (\( p < 0.05 \)) rightward shift, defined by a comparison between real and surrogate distributions by the Kolmogorov-Smirnov test. While mPFC \( \Delta V_m \) distributions at two HPC cell synchronizations (\( N_{sync} = 2 \)) were indistinguishable from chance level in the majority (84.6%) of datasets (\( n = 13 \) mPFC neurons), the significant effects tended to be more prominent as the number of synchronized HPC cells increased (Figure 2C; 37.5% [3/8], 50.0% [3/6], and 66.6% [2/3] for \( N_{sync} = 3, 4, \) and 5, respectively; no multiple comparisons were applied). These significant results were also observed when statistical tests were performed for comparisons between the distributions of mPFC \( \Delta V_m \) in a post-event 0-to-150-ms window and those of the corresponding baseline mPFC \( \Delta V_m \) (Figure S4H). While connectivity patterns with the HPC differ between the prelimbic (PL) subregion and anterior cingulate cortex (ACC) (Heidbreder and Groenewegen, 2003; Jay and Witter, 1991), these significant effects were observed in both regions (Figure S4N). Consistently, several mPFC cells showed similar significant depolarizing shifts during HPC SWRs (\( n = 6 \) out of 17 cells from 15 rats with HPC SWRs; Figures S4D and S4E). The same analysis was performed with a pre-event 0-to-150-ms window assuming that mPFC neuronal activity precedes HPC synchronization events (Figure S4F) and a post-event 350-to-500-ms window assuming that HPC synchronization events influence mPFC neuronal activity at more remote time (Figure S4G). In these cases, the significant fractions of mPFC \( \Delta V_m \) distributions were prominently lowered (13.3% and 6.7%, respectively), confirming that HPC synchronization events preceded significant mPFC membrane potential changes. We thus chose the post-event 0-to-150-ms window in the following analyses.

The datasets shown in Figure 2C demonstrate that several mPFC neurons exhibited significant \( \Delta V_m \) distribution shifts in response to synchronization with relatively low numbers of synchronous HPC cells (e.g., \( N_{sync} = 3 \)), whereas the other mPFC neurons exhibited no significant shifts even at larger numbers of synchronous HPC cells (e.g., \( N_{sync} = 4–5 \)). To further examine whether these differences may be due to different numbers of samples or the variability of samples used to compute Figure 2C, we classified mPFC neurons into two types: (1) significant mPFC cells that had at least one significant plot for \( N_{sync} \) from 2 to 5 (\( n = 7 \) cells, shown in red lines in Figure S4I) and (2) non-significant mPFC cells that had no significant plots for all \( N_{sync} \) (\( n = 6 \) cells, shown in blue lines in Figure S4I). Between the two cell groups, no significant differences were found in the numbers of HPC synchronous events and the variance of mPFC \( \Delta V_m \) distributions for all \( N_{sync} \) (Figure S4J; \( p > 0.05 \), Tukey’s test). These results confirm that differences in the sensitivity to HPC cell synchronization across mPFC neurons are not simply explained by differences in the numbers and the variability of samples.

We next examined whether individual HPC synchronized spike patterns were associated with mPFC \( \Delta V_m \) using a linear regression analysis with a leave-one-out cross-validation (Figure 2D). HPC synchronization events with at least three spiking HPC cells were used as a predictor vector \( s \) to predict the corresponding mPFC \( \Delta V_m \). For each mPFC neuron, a prediction error (in mV) was computed as an average of differences between observed and predicted mPFC \( \Delta V_m \) over all events. To assess the significance of predictability, a prediction score was defined as a negative value of the Z score computed from 1,000 surrogate datasets in which the order of mPFC \( \Delta V_m \) target variables, was randomly shuffled across all HPC synchronization events (an example mPFC neuron is shown in Figure 2D, and an additional two mPFC neurons are shown in Figure 2F). Of 13 mPFC neurons from 13 rats (with >4 HPC cells), 5 mPFC neurons (from 5 rats) had a significantly positive prediction score >1.96 (\( p < 0.05 \)), while the predictability was not apparently related to the number of recorded HPC cells (Figure 2G). Neurons with significantly positive scores were observed in both the PL and ACC (Figure S4O). The same results were observed when surrogate datasets were created by shuffling the order of HPC spikes across synchronization events and maintaining the total number of spikes within each cell (Figure S4L) or by shuffling the order of HPC synchronization events and maintaining the total numbers of HPC events at individual \( N_{sync} \) (Figure S4M). In predictable datasets, 60.5% of HPC neurons had positive weighted coefficients (Figure 2H, \( n = 43 \) HPC cells from 5 rats), implying that these HPC neurons have depolarizing, rather than hyperpolarizing, effects on mPFC neuronal membrane potentials. No significant correlations were found between weighted coefficients and baseline firing rates of individual HPC neurons (\( R = -0.078, p = 0.57 \)). Taken together, these results demonstrate that membrane potential changes in some mPFC cells are predictable from the summation of weighed synchronized spike patterns of HPC cells. With the time windows of 0–150 ms before and 350–500 ms after HPC synchronization, mPFC \( \Delta V_m \) was not predictive (Figures S4F and S4G), again confirming the HPC-leading-mPFC directionality.

**Reactivation of HPC place cell changes induces mPFC depolarization**

The findings of the HPC-mPFC \( \Delta V_m \) relationship next led us to ask whether HPC cells encoding behaviorally relevant information more strongly affect mPFC \( \Delta V_m \) in subsequent quiescent periods. Distributions of mPFC \( \Delta V_m \) were constructed for different numbers of synchronized HPC place cells (Figure 3A). Overall, mPFC \( \Delta V_m \) was larger at the occurrence of HPC synchronization events with place cell spikes, compared to that without place cell spikes (Figure 3B; 0 versus 1, \( Z = 3.84, p = 3.6 \times 10^{-4} \); 0 versus \( \geq 2, Z = 3.22, p = 0.0039 \); Mann-Whitney U test followed by Bonferroni correction; \( p = 9.5 \times 10^{-5} \), Kruskal-Wallis test). No differences in mPFC \( \Delta V_m \) were found between HPC synchronization events with one place cell and with two or more place cells (1 versus \( \geq 2, Z = 0.18, p > 0.99 \)).
In addition, we tested the effects of HPC SWRs that contained or did not contain place cell spikes on mPFC $\Delta V_m$. The frequencies of HPC SWRs with and without place cells were $0.19 \pm 0.05$ Hz and $0.12 \pm 0.03$ Hz, respectively ($n = 13$ rats). Overall mPFC $\Delta V_m$ during HPC SWRs with place cell spikes was significantly larger than that without place cell spikes (Figures 3C and 3D; $Z = 2.28$, $p = 0.023$, Mann-Whitney U test). We next directly analyzed whether synchronous events including specific place cell pairs more strongly affected mPFC $\Delta V_m$ (Figures 3E and 3F). Computing the distributions of mPFC $\Delta V_m$ from all possible HPC cell pairs (showing more than four synchronized spikes during a patch-clamp recording period) revealed that synchronization of place cell pairs showed significantly larger depolarization shifts of mPFC $\Delta V_m$ than that of non-place cell pairs (Figure 3G; $n = 80$ and 27 cell pairs, $Z = 2.13$, $p = 0.033$, Mann-Whitney U test). Moreover, there was a significantly larger depolarization of mPFC $\Delta V_m$ at synchronization of place cell pairs with their inter-field distance <30 cm (close pair, $n = 57$ cell pairs), but not at the distance >60 cm (distant pair, $n = 23$ cell pairs), than that of non-place cell pairs (Figure 3G; close versus non-place, $Z = 2.66$, $p = 0.016$; distant versus non-place, $Z = 0.35$, $p > 0.99$, Mann-Whitney U test followed by Bonferroni correction; $p = 0.017$, Kruskal-Wallis test). These significant effects were not observed when time windows to detect HPC synchronization events were shortened to 50 ms or shorter. These results suggest that reactivation of HPC place cells with overlapping spatial representations (Kudrimoti et al., 1999; Lee and Wilson, 2002; O’Neill et al., 2008; Wilson and McNaughton, 1994) exerts stronger synaptic influences on downstream mPFC neurons than those with nonoverlapping representations.

**Reactivation of HPC place cells in a novel environment induces mPFC depolarization**

During rest/sleep periods, especially after novel learning, the HPC-PFC circuits exhibit enhanced coordination of neuronal co-firing (O’Neill et al., 2008; Peyrache et al., 2009; Tang...
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DISCUSSION

There is ample evidence that the HPC-PFC communications are involved in memory functions (Eichenbaum, 2017; Tang and Jadhav, 2019), possibly by transferring information of neuronal activity patterns from the HPC to the PFC circuit for stabilization of memory traces (Euston et al., 2007; Jadhav et al., 2016; Maingret et al., 2016; Peyrache et al., 2009). In addition to the accumulating evidence, our study with concurrent HPC multunit recordings and mPFC whole-cell recordings revealed direct neurophysiological evidence of the substantial association of HPC synchronization events with mPFC subthreshold potentials (several millivolts in size). Considering the fact that even 1 mV depolarizing force was sufficient to produce postsynaptic neuronal spikes (Ikegaya et al., 2013), we find that the functional neurotransmission is a possible neurophysiological basis for the coordinated activation of spike trains across the HPC-PFC circuits (Benchenane et al., 2010; Jadhav et al., 2016; Peyrache et al., 2009; Shin et al., 2019). Interestingly, a subset of, but not all, mPFC neuronal membrane potentials were specifically responsive to synchronous HPC spike patterns (Figures 2C and 2G). These observations suggest that the sensitivity of mPFC neurons to HPC spike activity is heterogeneous, possibly due to differences in their anatomical and physiological properties, such as functional connectivity with the HPC and intrinsic excitability.

We note that our results showed a correlative, but not causal, relationship between HPC spike synchronization and mPFC membrane potentials. One possible scenario is that both the HPC and the mPFC activity might be induced by a common external drive from the other brain regions not measured in our study. Another point to note is that our results do not imply monosynaptic connections from the HPC to the mPFC. Considering the anatomical observations that dorsal HPC neurons send direct projections to the mPFC (Cenquizca and Swanson, 2007; Jay and Witter, 1991), the HPC-mPFC link we observed at the subthreshold level is likely mediated by indirect polysynaptic routes through the intermediate and ventral HPC having strong direct projections to the mPFC (Cenquizca and Swanson, 2007; Hoover and Vertes, 2007; Spellman et al., 2015), the
nucleus reuniens of the thalamus, and the other neocortical areas (Ito et al., 2015). These issues will be addressed in future experiments with the multisite electrophysiological recordings from brain regions. Tang et al. (2017) have demonstrated an arousal state-dependent modulation of mPFC neurons by HPC SWRs possibly due to the differences in neuromodulatory tone; excitation and inhibition of neuronal spikes occurred in almost equivalent proportions of mPFC neurons during awake SWRs (Jadhav et al., 2016), whereas excitatory modulation is more dominant in mPFC neurons during sleep SWRs (Siapas and Wilson, 1998). In our patch-clamp recording conditions, the head-fixed rats were in quiescent awake states. Considering our results that the HPC-PFC transmission was predominately depolarized, which possibly results in net increases in firing rates of mPFC neurons, the rats’ arousal states in this study might be closer to the sleep states observed by Tang et al. (2017). Together with the observation that awake HPC-PFC reactivation more accurately encoded behavioral experiences than sleep reactivation (Tang et al., 2017), the HPC-mPFC interactions observed in our study might become more reliable and contain more inhibitory effects under active awake conditions. The functional transmission in which behaviorally relevant information (e.g., similar spatial representations) encoded by HPC cell ensembles led to stronger depolarization in mPFC neurons might be necessary to generate coherent replay across the HPC-PFC circuits (Shin et al., 2019). Furthermore, the functional transmission in which novelty relevant information also led to stronger depolarization in mPFC neurons might implicate an efficient mechanism for mPFC neurons to preferentially respond to newly learned knowledge structures arising from the HPC (Shin et al., 2019; Tang et al., 2017). The learning-dependent synaptic influences might be useful to induce synaptic plasticity that would support long-term memory storage of new labile traces across the HPC-PFC circuits. Further studies are required to elucidate how mPFC neurons isolate information carried by specific novelty-related synapses from the other competing synaptic inputs. Given that timed spike sequences and neurotransmission are common neurophysiological mechanisms for all neurons in the brain, our findings are not just limited to the HPC-PFC circuits and could be extended to the other brain areas as a principle to achieve efficient information transfer across inter-regional neuronal ensembles.

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**SUPPLEMENTAL INFORMATION**

Supplemental Information can be found online at https://doi.org/10.1016/j.celrep.2021.108885.

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**AUTHOR CONTRIBUTIONS**

Y.N. and T.S. designed the study, Y.N. performed the surgery and acquired the electrophysiological data, and Y.N. and T.S. performed the analysis and prepared all figures. Y.I. supervised the project. T.S. wrote the main manuscript text, and all authors reviewed the main manuscript text.

**DECLARATION OF INTERESTS**

The authors declare no competing interests.

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**REFERENCES**


## STAR METHODS

### KEY RESOURCES TABLE

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<td><strong>Software and algorithms</strong></td>
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<td>MClust</td>
<td>By A. David Redish</td>
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### RESOURCE AVAILABILITY

**Lead contact**

Further information and requests for resources and reagents should be directed to and will be fulfilled by the Lead Contact, Takuya Sasaki (tsasaki@mol.f.u-tokyo.ac.jp).
Materials availability
This study did not generate any unique reagents. The CAD files for creating the feeding wheel and feeding port by 3D printers are available from the lead contact upon request.

Data and code availability
The original data are provided on Mendeley Data (https://dx.doi.org/10.17632/kc49ctr6yb.1). The codes are available from the lead contact upon request.

EXPERIMENTAL MODEL AND SUBJECT DETAILS
All experiments were performed with approval of the experimental animal ethics committee at the University of Tokyo (approval number: A30-72) and according to the NIH guidelines for the care and use of rats.

All Sprague Dawley male rats (3–5 weeks old) were purchased from SLC (Shizuoka, Japan). The rats were housed individually and maintained on a 12-h light/12-h dark schedule with lights off at 7:00 AM.

All behavioral experiments occurred in the dark phase. Following at least 1 week of adaptation to the laboratory, the rats were housed individually and reduced to 85% of their ad libitum weight through limited daily feeding. Water was readily available.

In total, 16 rats were trained in the U track task and used for recordings of local field potential (LFP) signals from the hippocampus (HPC). On days with recordings, 8 rats performed only a familiar U track task, and 8 rats first performed a familiar U track task followed by a novel U track task. All rats were then head-fixed under awake conditions. In addition, to confirm the physiological and morphological characteristics of mPFC neurons, whole-cell recordings of mPFC neurons were obtained from 9 rats (Figure S2E). To confirm the animal’s awake states, LFP recordings from the mPFC were obtained from 3 rats (Figures S1C and S1D).

METHOD DETAILS
Behavioral training on a U-shaped track
Before surgery, the rat was trained daily for at least 3 days to perform a U-shaped track task (Figure 1A). On one training day, the rat was trained to run back and forth on a U-shaped track consisting of three 70 × 9 cm² alleyways (with small sides rising 0.5 cm above the surface of the arm, 29 cm elevated from the floor) to obtain a constant amount of ~0.2 mL of chocolate milk reward placed at the track end during a 10-15-min session.

This training was repeated daily for 10 min until the rat consumed the reward at least 30 times within a 10-min training period. The rat was maintained on a pedestal with a diameter of 20 cm outside the track for 10 min before and after the task. After achieving the aim in the training phase, surgery was performed.

Surgical procedures
Pictures of the experimental instruments used for surgery are shown in Figure S1A. A standard electrode assembly for multiunit recording, called a microdrive, was prepared as described previously (Jog et al., 2002; Kloosterman et al., 2009; Nguyen et al., 2009). The rat was anesthetized with isoflurane gas (2%–2.5%) and then fixed in a stereotaxic instrument with two ear bars and a nose clamp. An incision was made from the area between the eyes to the back of the head. A rectangular craniotomy with a size of 1.2 × 2 mm was performed above the right hippocampus (3.6 mm posterior and 3.0–5.0 mm lateral to bregma) using a high-speed drill, and the dura was surgically removed. Two stainless-steel screws were implanted in the bone above the cerebellum to serve as ground and reference electrodes. A microdrive that consisted of 8 independently movable tetrodes, which was created using a 3D printer (Form 2, Formlabs) (Aoki et al., 2019; Okada et al., 2017; Yagi et al., 2018), was stereotaxically implanted (Figure S1A). The tip of the electrode bundle was lowered to the cortical surface, and the electrodes were inserted 0.75 mm into the brain at the end of surgery. The electrodes were constructed from 17-µm-wide polyimide-coated platinum-iridium (90/10%) wire (California Fine Wire), and the electrode tips were plated with platinum to lower electrode impedances to 180–300 kΩ at 1 kHz. The microdrive was physically protected by a cone-shaped plastic cover (13 mm height, 13 mm diameter in the top circle, 30 mm diameter in the bottom circle). To reduce its weight, the plastic cover had 36 elliptical holes 4 mm in the major axis and 2 mm in the minor axis.

In addition to microdrive implantation, a craniotomy with a diameter of ~1.3 mm was performed above the mPFC (2.5–3.5 mm anterior and 1.0–1.5 mm lateral to bregma). The dura was not removed during this procedure. To physically protect the craniotomy, polyimide tubing (3.5 mm height, 1.42 mm diameter) was vertically implanted on the craniotomy above the dura (Figure S1A). In addition, a quadrant-shaped plastic cover (~20 mm size, 5 mm height), which was created using a 3D printer, was placed on the skull surrounding the craniotomy, which protected the craniotomy from dental cement invasion and served as a pool for placing a ground electrode during subsequent patch-clamp recordings.

Finally, all of the wires, the Microdrive, and the cover were secured to the skull using stainless-steel screws and dental cement. Following surgery, the rat was housed individually in a transparent Plexiglass cage with free access to water and food for at least 3 days. After recovery from surgery, food was restricted to 85% according to their body weight.
Adjusting electrode depth

After the surgery, the rat was connected to the recording equipment via Cereplex M (Blackrock), a digitally programmable amplifier, close to the rat’s head. The output of the headstage was conducted via a lightweight multiwire tether to the Cereplex Direct recording system (Blackrock). Electrode turning was performed while the rat rested on the pedestal. The electrode tips were advanced slowly 25–250 μm per day for 10–17 days until spiking cells were encountered in the CA1 or CA2 layer of the hippocampus, which was identified on the basis of LFP signals and single-unit spike patterns. Once the tetrodes were adjacent to the cell layer, as indicated by the presence of low-amplitude multiunit activity, tetrodes were settled into the cell layer for stable recordings over a period of several days.

During the several days of this turning period, the rat was again trained, similar to the presurgery trainings. This postsurgery training lasted for at least 10–17 days before performing electrophysiological recording. Postsurgery training was performed with the recording headstage and cable attached to the rat’s head so that the rat became familiar with the recording conditions.

In addition, during this turning period, the rat was trained to habituate for subsequent patch-clamp recordings, as described previously (Lee and Lee, 2017). The rat’s head was stereotaxically fixed using a plastic headplate and left undisturbed for ~10 min on the first day (Figure S1B). A chocolate milk drop was sometimes provided to the fixed rat. The time of habituation was gradually increased to 30 min over the course of 10–17 days. This habituation training commenced until the rat sat quietly for several minutes without movement.

Electrophysiological recording in U track tasks

Electrophysiological data recordings during the U track task began after the rats again achieved the aim as in the postsurgery training phase, and stable well-separated unit activity was identified in the hippocampus. On a recording day, the rat was first maintained on the pedestal outside the track for 10 min, termed a pre-rest session, before and after the task. The rat then performed the U track task for 10–15 min. As the behavioral paradigm was completely identical to that of the training phases, this session was termed a familiar U track session. In some cases, the U track was rotated counterclockwise by 90 degrees without changing any external cues. As this positioning of the track was novel to the rats, this session was termed a novel U track session.

LFP recordings were sampled at 2 kHz and filtered between 0.1 and 500 Hz. Unit activity was amplified and bandpass filtered at 600 Hz to 6 kHz. Spike waveforms above a trigger threshold (60 μV) were time-stamped and recorded at 30 kHz for 1.6 ms. To monitor the rat’s moment-to-moment position, a near-infrared reflection sticker was attached to the microdrive on the animal’s head, and the position of the sticker was tracked at 25 Hz using an infrared camera (MCM-303NIR, Gazo, Japan) attached to the ceiling, which was sampled by a laptop computer.

In vivo patch-clamp recordings

After the U track tasks, the rat was fixed to the stereotaxic apparatus, as in the training habituation. Lidocaine solution (0.05 mg/kg, ~1 ml) was applied to the pool surrounded by the plastic cover above the mPFC craniotomy as an analgesic. The polyimide tubing/30-gauge stainless needle. Through the hole, a borosilicate glass pipette (4.0–7.0 MOhm), tilted at an angle of 10–15° to the posterior side, was lowered slowly to the mPFC, including the prelimbic or infralimbic cortex, at a depth of 750–3600 μm from the cortical surface (Figure S1B). Whole-cell recordings were obtained from neurons in these areas. The intrapipette solution consisted of the following reagents: 135 mM K-glucuronate, 4 mM KCl, 10 mM HEPES, 10 mM, Na2-phosphocreatine, 4 mM Mg-ATP, 0.3 mM Na3-GTP, 0.3 mM EGTA, and 0.2% bovine serum albumin. The solution was adjusted to pH 7.3 and 285–289 mOsm. The signal was amplified with a MultiClamp 700B, analyzed with pCLAMP10.1 (Molecular Devices, Union City, CA) and digitized at 20 kHz. At the beginning of each experiment, depolarizing and hyperpolarizing 1000-ms rectangular currents from −200 to +350 pA were injected into the cell at steps of 50 pA to characterize the cell’s intrinsic properties and spike responses. In the whole-cell current-clamp configuration, current steps (1000 ms) were applied; only cells that showed typical regular-spike characteristics of principal cells were selected (Figure S2E). The liquid junction potential was nulled offline. Cells were discarded when the series resistance exceeded 75 MΩ or the mean resting potential exceeded −50 mV. Moreover, recordings were truncated when the spike peak decreased below ~10 mV or the resting potential increased by more than 40 mV from its value at the onset of the recording. Throughout this recording process, no signs of painful behavior were observed. Under awake conditions, one and two cells were recorded from 14 and 2 rats, respectively.

Histological analysis to confirm tetrode locations and patch-clamped cells

After patch-clamp recordings, the rat received an overdose of urethane and was perfused intracardially with 4% paraformaldehyde in phosphate-buffered saline (PBS) (pH 7.4) and decapitated. To aid the reconstruction of electrode tracks, the electrodes were not withdrawn from the brain until 12 hours after perfusion. After dissection, the brain was fixed overnight in 4% PFA and then coronally cut into two tissues, one containing the prefrontal cortex and the other containing the hippocampus. The tissue containing the prefrontal cortex was sliced coronally at a thickness of 100-150 μm in PBS using a vibratome (Dosaka). The slices were incubated with 2 μg/ml streptavidin-Alexa Fluor 594 conjugate and 0.2% Triton X-100 for 6 hours, followed by incubation with 0.4% NeuroTrace 435/455 blue fluorescent Nissl Stain (Thermo Fisher Scientific: N21479) overnight. The slices were analyzed with an FV1200 (Olympus, Tokyo, Japan) confocal system under 20× and 40× objectives. Z series images were collected with 1.14-μm steps, and 4 Z sections (1 μm thick) were stacked using ImageJ (NIH). The other tissue containing the hippocampus was equilibrated with a sequence of 20%
sucrose and 30% sucrose in PBS. Frozen coronal sections (100-150 μm) were cut using a microtome, and serial sections were mounted and processed for cresyl violet staining. For cresyl violet staining, the slices were rinsed in water, counterstained with cresyl violet, and coverslipped with mounting agent (PARAmount-D, Falma). The positions of all tetrodes in the CA1 or CA2 regions were confirmed by identifying the corresponding electrode tracks in histological tissue. Recordings were included in the data analysis if the tetrode’s deepest position was in the cell layer.

**QUANTIFICATION AND STATISTICAL ANALYSIS**

**Spike sorting of hippocampal neurons**
Spike sorting was performed offline using the graphical cluster-cutting software MClust (Redish, 2009). Sleep recordings before and after the behavioral paradigms were included in the analysis to assure recording stability throughout the experiment and to identify hippocampal cells that were silent during behavior. Clustering was performed manually in 2D projections of the multidimensional parameter space (i.e., comparisons between waveform amplitudes, the peak-to-trough amplitude differences, and waveform energies, each measured on the four channels of each tetrode) (Figure S2C). Cluster quality was measured by computing the $L_{ratio}$ and the isolation distance (Schmitzer-Torbert et al., 2005). The $L_{ratio}$ was computed by the original equation, proposed by Schmitzer-Torbert et al. (2005), not normalized by the total number of spikes recorded on the tetrode. A cluster was considered as a cell when the $L_{ratio}$ was less than 0.30 and the isolation distance was more than 15 (Figure S2D; average $L_{ratio}$ was 0.113 ± 0.007 and average isolation distance was 34.7 ± 2.9 in 135 isolated cells). In the auto-correlation histograms, cells with no clear refractory period (< 3 ms) were excluded from analyses (Csicsvari et al., 1999; Harris et al., 2000). In addition, in the cross-correlation histograms, putative cell pairs with a symmetrical gap around the center bins were considered to arise from the same cell and were merged. Finally, cells with spike waveforms longer than 300 μs and an average firing rate of less than 3 Hz throughout an entire recording period were considered putative excitatory cells and included in the analysis.

**Spatial firing patterns of individual hippocampal neurons**
For analyzing spike patterns, the animal's coordinates and the positions of spikes of individual cells were projected onto a centerline of alleyways corresponding to each trajectory. The average firing-rate distribution on each trajectory (“R1 to R2” or “R2 to R1”) was separately computed along the projected line by dividing the total number of spikes in each location bin (10 cm) by the total time that the rat spent in that bin. The location bins of the reward area were excluded from subsequent analyses as the duration the rat spent in these areas was considerably different from those elsewhere on the track. All firing-rate distributions were smoothed by a one-dimensional convolution with a Gaussian kernel with a standard deviation of one pixel (10 cm). A place cell in a task was defined as a cell based on the two following criteria: (1) the average firing-rate distribution on a trajectory in a session had a maximum firing rate of more than 1 Hz (i.e., the absolute maximum firing rate), and (2) the maximum firing rate exceeded 2 standard deviations (SDs) above the mean, where the SD and the mean were computed from the series of firing rates except the maximum firing rate in that distribution. For each place cell, a place field center was defined as the position giving the maximum firing rate in the distribution. Under this criterion, some place cells had one place field in either one of two trajectories, whereas the others had two place fields in both trajectories. The other cells that did not meet the criteria were classified as non-place cells. For a given place cell pair, the distance between the two place field centers was computed, termed the place field distance. Place cell pairs with place field distances less than 30 cm and more than 60 cm were classified as close and distant place cell pairs, respectively.

For each place cell identified in the novel task, spatial firing patterns were compared between the familiar and the novel task (Figure S2f). Place fields that shifted their field center with a distance of 20 cm or less and 30 cm or more across the two tasks were classified as “stable” and “remap,” respectively. Place fields that newly emerged in the novel task were classified as “appear.”

**Detection of HPC synchronized spikes and SWRs**
During patch-clamp recordings, synchronization events of HPC neuronal spikes were detected when two or more HPC neurons were simultaneously activated in a time window of 100 ms. The onset of HPC synchronization events was defined at the time point when the first spike was observed. To detect SWRs from HPC LFP signals, the electrode including the largest number of HPC pyramidal cells identified in the spike sorting process was used. The HPC LFP signal was bandpass filtered at 150–250 Hz, and the root mean-square power was calculated in the ripple band with a bin size of 20 ms. The threshold for SWR detection was set to 3 standard deviations (SDs) above the mean (Carr et al., 2011), unless otherwise specified. In Figure S4A, the threshold was set to 3–6 SDs above the mean. The onset of SWRs was marked at the point when the ripple power first exceeded 2 SDs above the mean.

**Detection of neocortical oscillations**
To detect slow waves, mPFC LFP signal was bandpass filtered at 1–10 Hz, and the root mean-square power was calculated with a bin size of 1 s. The power during an active wakefulness of 2 min was considered as a baseline power, and a slow wave was detected when the power exceeded 1.5 times of the baseline (Narikiyo et al., 2020). To detect delta oscillations, mPFC LFP signal was bandpass filtered at 2–6 Hz, and the root mean-square power was calculated with a bin size of 100 ms. A delta oscillation was detected when the power exceeded 2 standard deviations (SDs) above the mean of the power for 150–500 ms (Todorova and Zugaro, 2019). To detect spindle oscillations, mPFC LFP signal was bandpass filtered at 7–10 Hz, and the root mean-square power was calculated...
with a bin size of 20 ms. The threshold for spindle oscillation detection was set to 3.5 standard deviations (SDs) above the mean (Latchoumane et al., 2017). During awake head-fixed periods in the conditions of our patch-clamp recordings, no oscillations were detected as shown in Figures S1C and S1D.

Membrane potential changes in mPFC neurons during HPC synchronization

From mPFC patch-clamp recording data, membrane potential changes in the mPFC at the time of HPC synchronization or SWR events were computed. For all the following analyses, only HPC events that were temporally separated by more than 200 ms from prior SWR events were analyzed. This procedure excluded the second and subsequent events that were possibly involved in ripple bursts (Yamamoto and Tonegawa, 2017). For each HPC event, a difference in average mPFC membrane potentials between 0–150 ms after and 50–200 ms before the HPC event was computed, termed mPFC \( \Delta V_m \), unless otherwise specified. In Figure S4, mPFC \( \Delta V_m \) was computed as a difference in mPFC \( V_m \) between 0–150 ms and 200–350 ms before HPC events (Figure S4F) and between 350–500 ms after and 50–200 ms before HPC events (Figure S4G). To assess whether a distribution of mPFC \( \Delta V_m \), was observed above chance level, a surrogate distribution was constructed with the same procedure from 1000 surrogate datasets in which the same mPFC \( \Delta V_m \) was extracted at random time points in the same dataset. The original distribution was considered to be significant when there was a significant difference between the original and surrogate distribution computed by the Kolmogorov-Smirnov test. In Figures S4D and S4E, the same analysis was applied to HPC SWRs instead of HPC synchronization. Here, 17 mPFC cells from 15 rats with more than 10 HPC SWRs were analyzed.

Prediction of mPFC membrane potential changes from HPC synchronized spike patterns

Using linear regression analysis, we predicted the mPFC \( \Delta V_m \) of a place cell during a patch-clamp period from synchronized spike patterns of HPC neuronal ensembles (Figures 2D–2G). Data with more than 4 HPC cells were analyzed (\( n = 13 \) mPFC cells from 13 rats). A predictor vector \( s \) was defined as spike patterns of all HPC cells in individual HPC synchronization events with at least 3 spiking HPC cells, and a target variable \( v \) was set as the corresponding mPFC \( \Delta V_m \) of a whole-cell recorded mPFC cell. For each HPC synchronization event, a vector of weighted coefficients \( w \) was computed so that the weighted linear sum \( \Delta V_m \) was fitted against \( v \). In each HPC synchronization event, a leave-one-out cross-validation analysis was applied to examine the predictability of the target variable.

For more detail, for the \( l \)-th HPC synchronization event, a \((N+1)\)-dimensional predictor vector was defined as a population vector \( s_l \), the \( N \)-dimensional entries of which were the binary indexes representing the presence or absence of spikes (1 for one or more spikes, 0 for no spike) of individual HPC cells during the \( l \)-th HPC synchronization event, where \( N \) denotes the total numbers of HPC cells, and the \((N+1)\)-th entry was set at +1 as a constant term. For a whole-cell recorded mPFC neuron, a target variable \( v_l \) was set as the mPFC \( \Delta V_m \) during the \( l \)-th HPC synchronization event. A linear regression function was applied to estimate a linear relationship between a series of predictor vectors, \( S = (s_1, s_2, s_3, \ldots, s_L)^T \), and a series of target variables, \( v = (v_1, v_2, v_3, \ldots, v_L)^T \), where \( L \) denotes the total number of HPC synchronization events and is greater than \((N+1)\). The best \((N+1)\)-dimensional weighted vector \( w \) was mathematically computed as follows:

\[
\begin{align*}
  w &= S^* v, \\
  S^* &= \left(S^T S\right)^{-1} S^T.
\end{align*}
\]

To evaluate the predictability of the \( l \)-th target variable \( v_l \), leave-one-out cross-validation was performed by computing \( w \) from the dataset without \( s_l \) and \( v_l \). A predicted target variable \( \hat{v}_l \) was calculated as follows:

\[
\hat{v}_l = s_l^T w.
\]

The same analyses were repeated for all \( L \) HPC synchronization events, and a series of predicted variables \( v' \) were compared with the observed variables \( v \), as shown in Figure 2D. The accuracy of the prediction during the timescale of an entire recording session was assessed by computing a prediction error as an average absolute difference between the two variables, \( v \) and \( v' \). To evaluate the significance of a prediction error in real data, errors were computed with the same procedures from 1000 surrogate datasets created by shuffling the order of observed variables \( v \) across all HPC synchronization events (Figure 2D, bottom). A z-score of a prediction error was computed based on a distribution of 1000 prediction errors from 1000 surrogate datasets, and a prediction score for an mPFC neuron was defined as the negative value of the z-score. A prediction score of 1.96 was set as a threshold to define cells with significantly positive prediction scores \((p < 0.05)\) as this z-score represents the approximate value suggesting 95% confidence intervals in the normal distribution of surrogate datasets.

Statistics

All data are presented as the mean ± standard error of the mean (SEM) and were analyzed using MATLAB. Comparisons between real and surrogate distributions were analyzed by the Kolmogorov-Smirnov test in Figure 2. Comparisons between two datasets were analyzed by the Mann-Whitney U test in Figures 3 and 4. Multiple group comparisons were performed by Mann-Whitney U test followed by post hoc Bonferroni corrections after Kruskal-Wallis test. The null hypothesis was rejected at the \( p < 0.05 \) level.